

Article

# Automatic detection and distinction of retinal vessel bifurcations and crossings in colour fundus photography

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**Abstract:** The analysis of retinal blood vessels present in fundus images, and the addressing of problems such as blood clot location, is important to undertake accurate and appropriate treatment of the vessels. Such tasks are hampered by the challenge of accurately tracing back problems along vessels to their source. This is due to the unresolved issue of distinguishing automatically between vessel bifurcations and vessel crossings in colour fundus photographs. In this paper, we present a new technique for addressing this problem using a convolutional neural network approach to firstly locate vessel bifurcations and crossings and then to classifying them as either bifurcations or crossings. Our method achieves high accuracies for junction detection and classification on the DRIVE dataset and we show further validation on an unseen dataset from which no data has been used for training. Combined with work in automated segmentation, this method has the potential to facilitate: reconstruction of vessel topography, classification of veins and arteries and automated localisation of blood clots and other disease symptoms leading to improved management of eye disease.

**Keywords:** medical image analysis, machine learning, convolutional neural networks, retinal imaging, retinal vessels, fundus photography, vessel classification

## 1. Introduction

Vascular conditions present a challenging public health problem as they become more common due to global ageing [1]. Vascular conditions are often life-threatening and blood vessel damage caused from common health issues such as diabetes, hypertension and strokes can lead to significant health complications. It is therefore of great importance to better understand and be able to manage such conditions. The retina is the only inner organ which can be directly imaged, using a fundus camera, and also serve as a “window” for the diagnosis of systematic diseases such as: cerebral malaria, stroke, dementia and cardiovascular diseases [2]. It is also significant that pathologies often affect veins and arteries differently. For example, in diabetic retinopathy, abnormalities typically occur in veins such

25 as venous beading which is a significant predictor to the sight-damaging proliferative stage of the  
26 condition. With the availability of imaging techniques such as colour fundus photography, fundus  
27 angiography and recent optical coherence tomography angiography, there is a significant need for  
28 automated vessel analysis techniques [3,4].

29 There has been a considerable amount of work, in recent years, aimed at the effective segmentation  
30 of retinal blood vessels in fundus photography, which is a prerequisite step for blood vessel analysis.  
31 Work such as [3–5] has been able to achieve increasingly improved segmentation of retinal vessels.  
32 However, a significant remaining challenge is to distinguish between vessel bifurcations and vessel  
33 crossings. A vessel bifurcation is where a mother vessel branches into two daughter vessels, whilst a  
34 vessel crossing is where one vessel passes over another but does not connect to it. This is important for  
35 tracking vessels, separating veins from arteries and providing for quantitative analysis of vasculature.

36 For example, we must be able to trace back along the vessel when a blood clot has been identified.  
37 The current inability to accurately identify vessel crossings after or during vessel segmentations  
38 hinders this. It is also important to monitor progress of a vessel after vein and artery occlusions;  
39 being able to identify and distinguish vessel crossings and bifurcations facilitates this. Automating  
40 the detection and classification of vessel bifurcations and crossings also allows us to aid clinicians  
41 in detecting vascular abnormalities. The vast amount of vessels and vessel junctions within the  
42 retina make this task a laborious one for clinicians; by automating the process we can save time for  
43 treatment while maintaining accuracy. The vasculature can be obtained through vessel tracking or  
44 pixel-based classification. Detecting bifurcations and crossings are critical to either of these vasculature  
45 reconstruction methods. The detected and classified vessel junctions can be used in combination with  
46 vessel segmentation, or used in vessel tracking methods to detect the source of irregular vasculature.

47 The previous work on vessel bifurcations and junctions has involved using orientation scores to  
48 detect bifurcations and junctions in retinal images[6]. In contrast to the method we proposed, which is  
49 a fully automated system that uses only the image to determine the diagnosis, the work in [6] required  
50 24 orientation processes for each image before training. However, the results in the paper show that  
51 the features within the image are extractable. There has also been similar orientation based work in  
52 [7,8].

53 For applications in image analysis and classification, Convolutional Neural Networks (CNNs),  
54 a branch of deep learning, has achieved state of the art results for many problems. The 1970's saw  
55 the introduction of network architectures being used to analyse image data [9]. These had useful  
56 applications and allowed challenging tasks, such as handwritten character recognition [10], to be  
57 achieved. Decades later, there were several breakthroughs in neural networks that lead to vast  
58 improvements in their implementation, such as the introduction of dropout [11] and rectified linear  
59 units [12]. These theoretical enhancements and the accompanying increase in computing power  
60 through graphical processor units (GPUs) meant that CNNs became viable for more complex image  
61 recognition problems. Presently, large CNNs are used to successfully tackle highly complex image  
62 recognition tasks with many object classes to an impressive standard.[13,14] The recent improvements  
63 in image recognition problems mentioned present an opportunity for more efficient and accurate  
64 methods of our vessel problem. CNNs are used in many of the current state-of-the-art image  
65 classification tasks including medical imaging. Hence, we use this method combined with expert  
66 segmented fundus images and skeletonisation [15][16] to detect and classify vessel bifurcations and  
67 crossings within fundus images.

68 There are many different architectures for neural networks. Recently residual networks have  
69 achieved impressive results on the highly competitive competition of ImageNet detection, ImageNet  
70 localisation, COCO detection, and COCO segmentation [17]. They were then widely used in the  
71 following 2016 ImageNet competition due to their impressive performance on general large data sets  
72 of small images; such as the MNIST [18] dataset for handwritten digits 0-9 and CIFAR-10 [19], a dataset  
73 of 10 classes of colour images. This network learns from the residual of the identity of the previous  
74 layer of a new layer in order to learn features more effectively. This makes the network ideal for our

75 patch based method as the higher level features can distinguish between the background of the retina  
76 and the bifurcations and crossings. Hence, the Res18 network structure, containing 18 residual layers,  
77 was used in the CNNs throughout this paper.

78 In this paper, we present a new hierarchical approach, that utilises deep learning, to first  
79 automatically determine the locations of blood vessel bifurcations and crossings in colour fundus  
80 images, and then to distinguish between vessel bifurcation and crossings. We employ an available  
81 segmentation of the vessel structure, although an automatic segmentation procedure could be  
82 incorporated, to identify points along blood vessels. Annotated image datasets with identified vessel  
83 bifurcations and crossings aid our deep learning framework as we use a supervised learning method  
84 to solve this image recognition problem. From the original fundus images of the DRIVE dataset we  
85 created small patches of images using a skeletonisation of the vessels. We use a convolutional neural  
86 network approach which is trained on some of the patches of the fundus images using the expert  
87 ground truth for optimization. A matching network architecture is then used and trained to learn new  
88 convolution filters to distinguish between vessel bifurcations and crossings. The results is a novel  
89 method which is capable of identifying and classifying vessel bifurcations and crossings without user  
90 intervention.

91 The rest of this paper is organised as follows. In §2, we present our new automatic approach  
92 for locating and identifying crossings and bifurcations of retinal vessels, in §3 we demonstrate that  
93 proposed method yields robust, state-of-the-art results and in §4 and §5 we present our conclusions  
94 and discuss future work. This paper is an extension of the paper [20] extended and more substantial  
95 results and a refined method for accuracy. The figures used are cited throughout.

## 96 2. Methods

97 Firstly we identifying patches of fundus images  $z(\mathbf{x})$ . During our experiments we found that the  
98 optimal size for both performance and collection of the patches was 21 by 21 pixels. All of the patches  
99 used throughout this method were of this size. We make use of available vessel segmentations given  
100 as binary functions defined on the domain, and perform a skeletonisation process on this domain.  
101 The patches are then produced along the skeleton so that each contains some of vessel structure.  
102 Furthermore, after creating the patches we train our Res18 convolutional neural network to identify  
103 the patches which include either a bifurcation or a crossings. The res18 neural network contains 18  
104 convolutional layers learned using the residual of the previous convolutional layer as in [17]. The  
105 network contains 11,181,570 trainable weight parameters for optimization and the architecture layout  
106 can be found in the supplementary material. Another network with the same architecture is then  
107 trained on the patches that have been graded to have bifurcations and crossings to distinguishing the  
108 type of vessel junction located.

109 We tested the ability of our algorithm using 40 images from the DRIVE database with manual  
110 segmentations [4]. We also studied the variability between grading and how this relates to the trained  
111 network for each grader. The data split was 30 images for training the neural networks, leaving 10  
112 for testing. While this may seem a small number for a machine learning approach, our patch based  
113 method means that the images generated for training numbered more than 100,000 providing sufficient  
114 data. Ground truth annotations of vessel crossings and bifurcations were provided by two graders (G1  
115 and G2).

### 116 2.1. Datasets

117 The images used to implement our framework are from the Digital Retinal Images for Vessel  
118 Extraction (DRIVE) database with manual segmentations [4]. The images in the DRIVE dataset were  
119 obtained from a diabetic retinopathy screening program in The Netherlands. The images were acquired  
120 using a Canon CR5 non-mydratic 3CCD camera with a 45 degree field of view (FOV) using 8 bits per  
121 colour plane at 768 by 584 pixels.

122 Moreover, we use the IOSTAR dataset [6,21] for testing the robustness of the method. Our  
 123 networks are trained on the DRIVE Dataset, but all of them are tested on the unseen IOSTAR dataset  
 124 for further validation. The IOSTAR dataset is made of the images taken with EasyScan camera  
 125 (provided by i-Optics B.V., the Netherlands). The original images have a resolution of 1024 by 1024  
 126 ( $14 \mu\text{m}/\text{px}$ ), and a 45 degree field of view. For the moment, vessels, bifurcations and crossings of 24  
 127 images have been annotated and corrected by two different experts, the same experts that graded the  
 128 DRIVE dataset. For testing on the IOSTAR dataset, which has the same field of view as DRIVE, the  
 129 images were resized using bilinear interpolation to the dimensions of the DRIVE images. Patches were  
 130 then extracted in the same way with both datasets to allow for fair comparison purposes. This process  
 131 can be used to compare with any dataset of varying image size.

132 The datasets were graded separately by 3 expert graders to compare variability between the  
 133 networks and between the graders themselves. The graders labelled bifurcations by clicking as close  
 134 to the centre of the junction as possible. This allowed for it to be a simple operation so that the graders  
 135 focus could remain on image.

## 136 2.2. Skeletonisation and patch extraction

137 We consider patches of the fundus images centred along the segmented vessels. In order to restrict  
 138 the number of patches for training to a manageable number, and reduce bias, we aim to reduce to  
 139 segmentation of the vessels to a skeleton and consider regions centred only on these points. We achieve  
 140 this by performing a skeletonisation of the level set function  $\phi(\mathbf{x})$  for each image. We convolve the  
 141 level set function with the kernels:

$$\kappa_1^j(\alpha^1) = r_j \begin{pmatrix} 0 & 0 & 0 \\ \alpha_1^1 & 1 & \alpha_2^1 \\ 1 & 1 & 1 \end{pmatrix}, \quad \kappa_2^j(\alpha^2) = r_j \begin{pmatrix} \alpha_1^2 & 0 & 0 \\ 1 & 1 & 0 \\ \alpha_2^2 & 1 & \alpha_3^2 \end{pmatrix}, \quad (1)$$

142 where  $r_j$  denotes rotation of the matrix by a multiple  $j$  of  $\pi/2$  radians and  $\alpha^1 = (\alpha_1^1, \alpha_2^1)^\top \in \Psi^2$ ,  
 143  $\alpha^2 = (\alpha_1^2, \alpha_2^2, \alpha_3^2)^\top \in \Psi^3$  where  $\Psi = \mathbb{Z} \cap [0, 1]$ . We thin the segmentation of the vessels by removing  
 144 the points which are centred on regions matching the above filters. That is, we set such points as  
 145 background points. We achieve this by iterating:

$$\begin{aligned} \varphi^{\ell+1} &= \mathcal{F}_{i,j}(\varphi^\ell), \quad \ell = 0, 1, \dots, \quad \varphi_0(\mathbf{x}) = \phi(\mathbf{x}) \\ \mathcal{F}_{i,j}(\varphi) &= \varphi - 1 + H \left( \left( \kappa_i^j(\alpha^i) * \varphi - \sum \kappa_i^j(\alpha^i) \right)^2 \right), \end{aligned} \quad (2)$$

146 beginning with  $l_0^1 = 0$  and cycling through  $i \in \{1, 2\}, j \in \{0, 1, 2, 3\}$ .

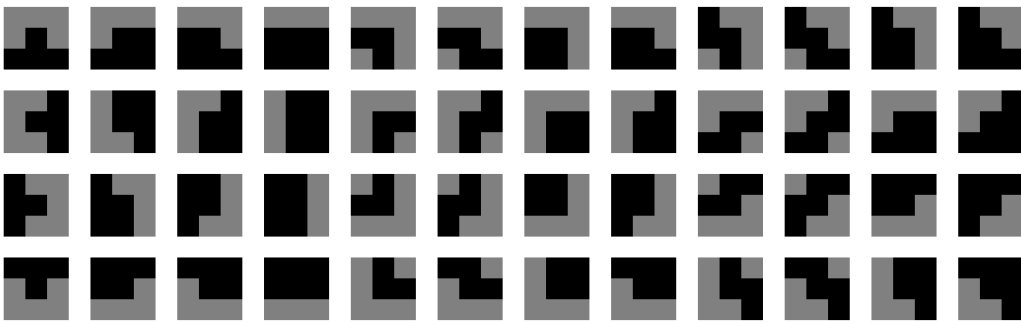


Figure 1. Kernel functions for skeletonisation [20] Reproduced with permission

147 Following this, we extract the patches by cropping the image  $z(\mathbf{x})$  to  $21 \times 21$  pixel windows  $\Theta_{\mathbf{p}}$   
 148 centred on points  $\mathbf{p}$  in the set  $Y$  of points considered the foreground of the skeletonised vessel map.

149 The patch size was selected so that bifurcations, and crossings and branches, in the vessel would fit  
 150 within one patch. The patches are given by:

$$\Theta_{\mathbf{p}} = \{\mathbf{q} \in \Omega \mid |\mathbf{p} - \mathbf{q}| \leq 10\}, \quad \mathbf{p} \in Y = \{\mathbf{p} \in \Omega \mid \varphi(\mathbf{p}) = 1\}.$$

151 In the training stage, the set of patches ( $\Theta$ ) of the images in the training set are used to train the neural  
 152 network to identify whether a bifurcation or crossing is contained in the image patch. In the test stage,  
 153 the trained CNN classifies the patches accordingly. This step is described below.

### 154 2.3. Junction distinction - CNN $\mathbb{C}_1$

155 To identify the vessel bifurcations and crossings within the patches created we train our CNN  
 156 on a high-end Graphics Processor Unit (GPU). The large random access memory of the Nvidia K40c  
 157 means that we were able to train on the whole dataset of patches at once. The Nvidia K40c contains  
 158 2880 CUDA cores and comes with the Nvidia CUDA Deep Neural Network library (cuDNN) for GPU  
 159 learning. The deep learning package Keras [22] was used alongside the Theano machine learning back  
 160 end to implement the network. After training, the feed forward process of the CNN can classify the  
 161 patches produced from a single image in under a second.

162 We used the Res18 network architecture [17] as deep levels of convolution were required to  
 163 distinguish the vessel junction type in our small patches. The residual layers incorporate activation,  
 164 batch normalisation, convolutional, dense and maxpooling layers. We also use  $L^2$  regularisation to  
 165 improve weight training. There were approximately 100,000 patches for training and 30,000 for testing  
 166 in the junction distinction problem. The classes were weighted as a ratio of junction to background  
 167 due to the fact that bifurcations and crossings in the training and testing patches were sparse at a ratio  
 168 of 1:39. The network was optimised using Adam stochastic optimisation for backpropagation [23].  
 169 The network was trained to classify the patches to give a binary classification of either vessel junction  
 170 or background. Gaussian initialisation was used within the network to reduce initial training time.  
 171 The loss function used for the optimisation was the widely used categorical cross-entropy function.  
 172 Training was undertaken until reduction of the loss plateaued to obtain optimal results.

### 173 2.4. Locate the centres

174 Following the neural network classification, which tell us if a bifurcation or crossing is contained  
 175 within a patch, we aim to find the locations of the points. We achieve this by forming the cumulative  
 176 sum image:

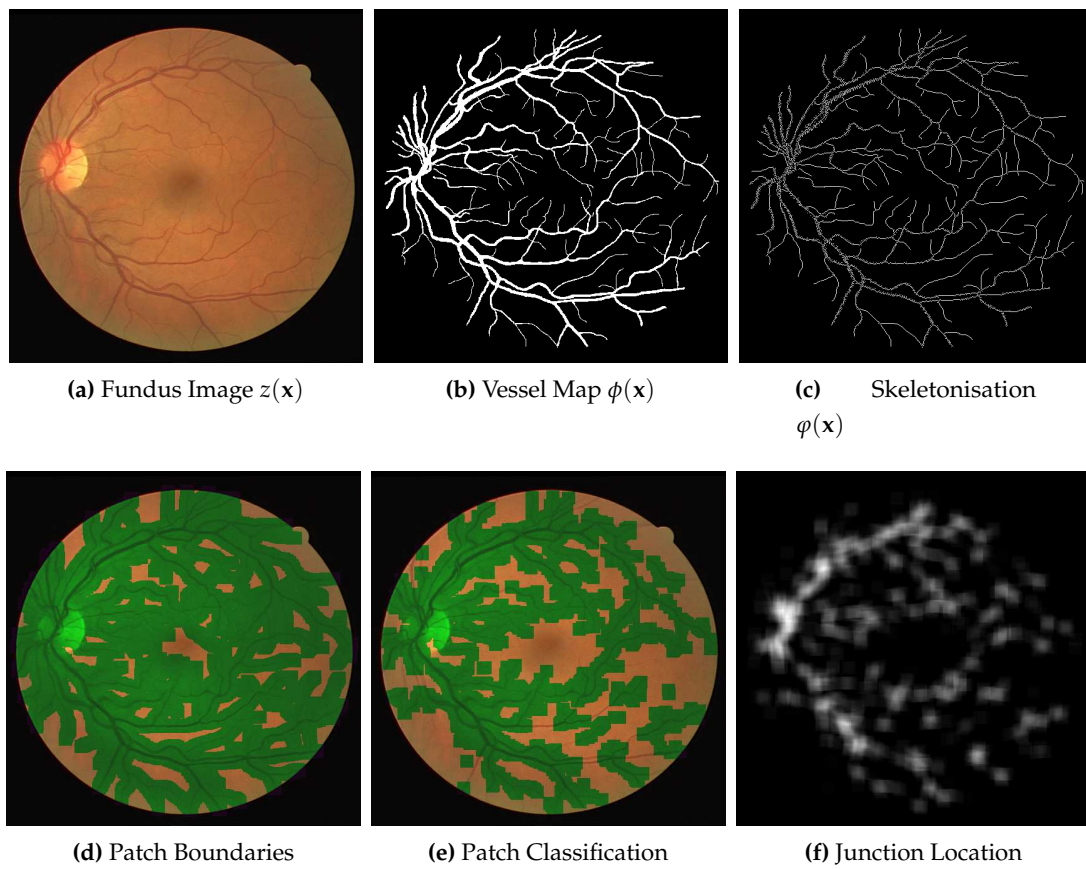
$$t(\mathbf{q}) = \sum_{\mathbf{p} \in Y} s^{\mathbf{p}}(\mathbf{q}, l), \quad s^{\mathbf{p}}(\mathbf{q}, l) = \begin{cases} l_{\mathbf{p}}^1 & \text{if } \mathbf{q} \in \Theta(\mathbf{p}) \\ 0 & \text{otherwise} \end{cases} \quad (3)$$

177 and taking the local maxima  $\mathbf{r} \in Y$  as points of interest. We then aim to determine whether points are  
 178 at crossings or bifurcations.

### 179 2.5. Junction Classification $\mathbb{C}_2$

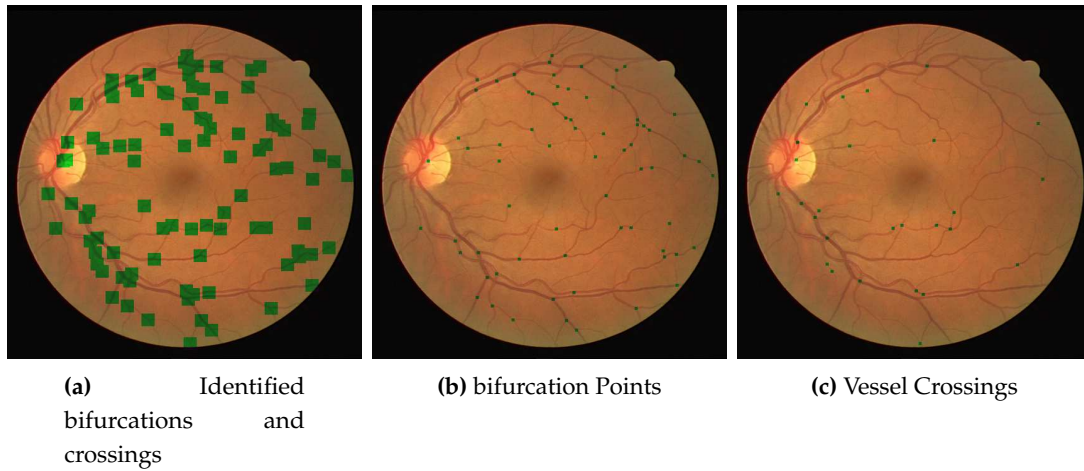
180 We extract the patches  $\Theta(\mathbf{r})$  and use these to train a neural network to distinguish between  
 181 crossings and bifurcations. The second neural network was trained with the Res18 architecture, like  
 182 the first. Using a relatively small training set of patches, as from our images the majority of patches  
 183 did not contain bifurcations and crossings, we trained our network in similar fashion to that used in  
 184 the previous step. Weighted classes were introduced again to cater for the imbalance, in that images  
 185 from the bifurcation class were substantially more prominent than that of the cross class.

186 Depending on the patch method there were around 800-2500 patches containing a junction  
 187 that was used for training. In all methods there were approximately twice as many junction  
 188 patches containing bifurcation vessels compared to patches containing vessels crossing. Training

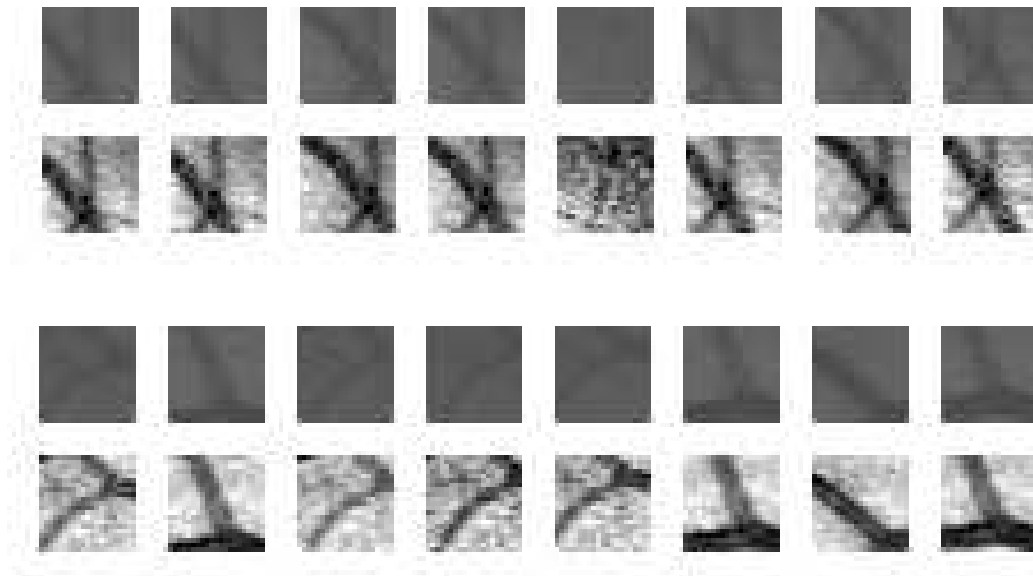


**Figure 2.** Example outcomes of first part of algorithm: locating bifurcations and crossings. [20]  
Reproduced with permission

189 was performed until a plateau in the reduction of the loss function was reached indicating no further  
 190 improvement.



**Figure 3.** Example outcomes of second part of algorithm: classifying bifurcations and crossings as bifurcations and crossings. [20] Reproduced with permission



**Figure 4.** Example of  $\mathbb{C}_2$  input. Rows 1 and 2 (resp. 3 and 4): training patches with crossings (resp. bifurcations) and their enhanced counterparts for presentation. The neural networks were able to achieve good results using the patches without enhancement. [20] Reproduced with permission

### 191 3. Results

We present our results on a patch by patch basis as well as in the fundus image form with vessel bifurcations and splittings labeled. The patch detection and classification information is then used to in a probability map type reconstruction of the fundus image to produce the final appropriate vessel bifurcations and splittings, as demonstrated in Figures 5 and 6. Here we present both the patch accuracy results and the final classified and vessel type distinguished images. We measure sensitivity, specificity and accuracy of the final image-based result as follows. Since the region of a junction is not

restricted to a single point, we allow a region  $r(x, y)$  of 10 pixels either side of an annotated point at  $(x, y)$  to be considered the correct region. That is, we split each image domain  $\Omega$  into two sets

$$\Omega_1 = \{(x, y) | j \in r(x, y)\}, \quad \Omega_2 = \Omega \setminus \Omega_1$$

192 where  $j$  denotes a junction point location.  $\Omega_1$  is considered the true (junction) set and  $\Omega_2$  is considered  
193 the background set. We then calculate error measures based on this and report the mean measures.

194 For validation we used the test images from the DRIVE dataset. Furthermore, we used the  
195 separate IOSTAR dataset, and another expert grader (G3), for testing and comparison of the patch  
196 detection and classification method. We show in Table 1 and 2 the results of training our neural  
197 networks on the data provided by graders 1, 2 and 3. In each case, we use patches extracted from 30  
198 images from the DRIVE dataset to train our network. This relates to 101,416 patches of vessel junctions  
199 and 216,756 other patches. From the 101,416 patches there are 67,650 patches of vessel crossings and  
200 33,766 patches of vessel bifurcations. This network is then tested by using our network to classify  
201 patches from the remaining ten images of the DRIVE dataset. This relates to 72,980 non-vessel patches  
202 and 31,026 vessel patches of which 9,176 are vessel crossings and 21,850 are vessel bifurcations. We  
203 compare the results with the annotations provided by the grader in question, achieving high accuracies  
204 of 0.76, 0.76 and 0.77 for graders 1, 2 and 3 respectively. Furthermore, we use the trained network to  
205 classify images from the IOSTAR dataset, comparing with the annotations provided. With each trained  
206 network, the accuracy is lower for this unseen dataset, but the sensitivity is retained. The IOSTAR  
207 dataset gave us 132,064 non-vessel junction patches and 52,878 vessel junction patches with 14,228  
208 vessel crossings and 38,650 vessel bifurcations. Following the detection, we resolve the patch-based  
209 results into the original images in order to identify individual junctions and to measure the detection  
210 performance for each image. Table 3 and 5 shows the results obtained from the networks trained by  
211 the first annotations of grader 2 and grader 3 and tested on the 10 remaining test images of the DRIVE  
212 dataset. The results were compared with the annotations of grader 1 (G1A1), the first and second  
213 annotations of grader 2 (G2A1 and G2A2) as well as the first and second annotations of grader 3 (G3A1  
214 and G3A2). Excellent performance of 81% is achieved for the network trained and tested on grader  
215 2's first annotation. The result is similar when comparing to the other graders. Good performance  
216 of 74% is also achieved for the network trained and tested on grader 3's first annotation with similar,  
217 and even improved, results when comparing to other annotations. We retain good accuracy for the  
218 classification task, as shown in Table 4 and Figures 7 and Figure 8, achieving accuracies of  $\geq 0.70$   
219 for distinguishing between detected vessel crossings and bifurcations. The results were a little lower for  
220 the IOSTAR dataset but this, and the detection results, may be improved by including some of this  
221 data in the training of the networks.

**Table 1.** CNN-based Detection results

<b>Training on Grader 1</b>			
<b>Test Set</b>	<b>Accuracy</b>	<b>Sensitivity</b>	<b>Specificity</b>
G1A2	0.7622	0.7398	0.7714
IOSTAR	0.7349	0.5225	0.8199
G1A1	0.8055	0.6244	0.8688
<b>Grader 2</b>			
<b>Test Set</b>	<b>Accuracy</b>	<b>Sensitivity</b>	<b>Specificity</b>
G2A2	0.7620	0.7472	0.7681
IOSTAR	0.6302	0.7639	0.5767
G1A1	0.7537	0.7704	0.7479
<b>Grader 3</b>			
<b>Test Set</b>	<b>Accuracy</b>	<b>Sensitivity</b>	<b>Specificity</b>
G2A2	0.7654	0.7408	0.7756
IOSTAR	0.6586	0.7466	0.6234
G1A1	0.7574	0.7664	0.7543



**Table 2.** Confusion Matrices for CNN-based Detection results. BG denotes background, JC denotes junctions. True labels are along rows, predicted along columns.

<b>Training on Grader 1</b>								
<b>G1A2</b>	<b>BG</b>	<b>JC</b>	<b>IOSTAR</b>	<b>BG</b>	<b>JC</b>	<b>G1A1</b>	<b>BG</b>	<b>JC</b>
<b>BG</b>	56732	7926	<b>BG</b>	108284	25248	<b>BG</b>	66969	10113
<b>JC</b>	16811	22537	<b>JC</b>	23780	27630	<b>JC</b>	10115	16809
<b>Grader 2</b>								
<b>G2A2</b>	<b>BG</b>	<b>JC</b>	<b>IOSTAR</b>	<b>BG</b>	<b>JC</b>	<b>G1A1</b>	<b>BG</b>	<b>JC</b>
<b>BG</b>	56847	7701	<b>BG</b>	76161	12484	<b>BG</b>	57651	6181
<b>JC</b>	17056	22762	<b>JC</b>	55903	40394	<b>JC</b>	19433	20741
<b>Grader 3</b>								
<b>G2A2</b>	<b>BG</b>	<b>JC</b>	<b>IOSTAR</b>	<b>BG</b>	<b>JC</b>	<b>G1A1</b>	<b>BG</b>	<b>JC</b>
<b>BG</b>	57039	7896	<b>BG</b>	82329	13399	<b>BG</b>	58143	6290
<b>JC</b>	16504	22567	<b>JC</b>	49735	39479	<b>JC</b>	18941	20632

**Table 3.** Image-based Detection results

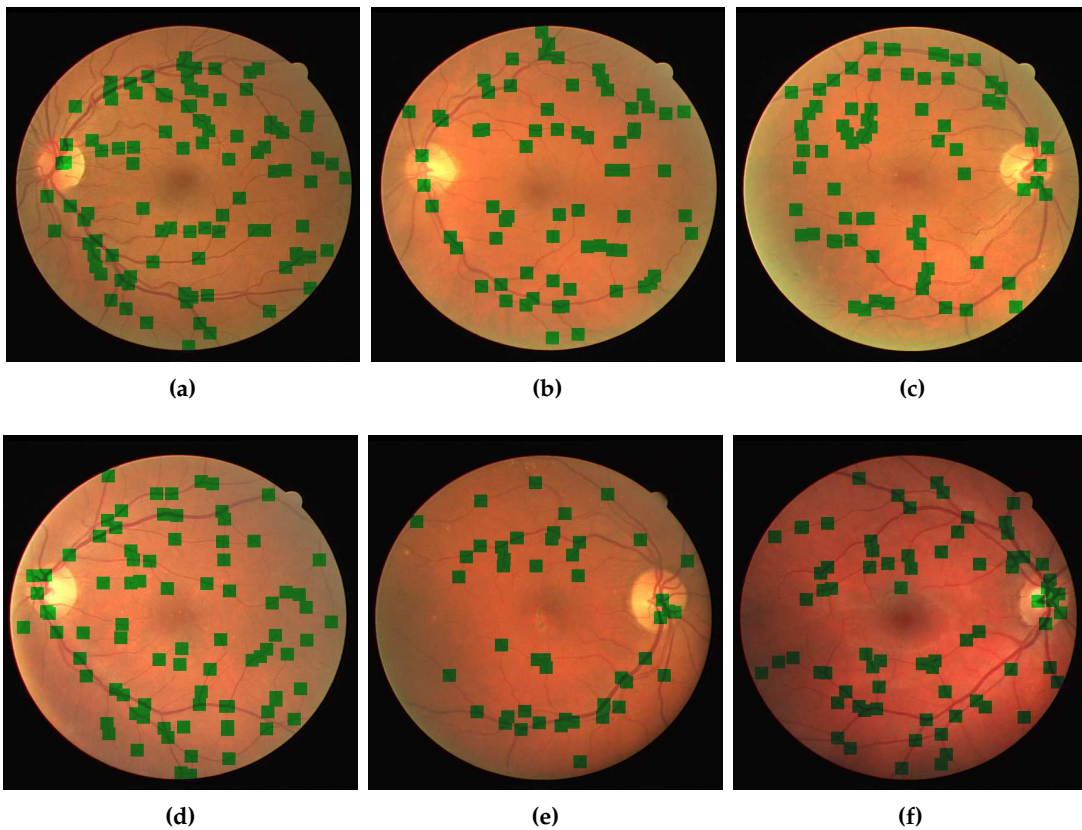
<b>Grader 2</b>						
<b>Tested on</b>	G1A1	G2A1	G2A2	G3A1	G3A2	
Sensitivity	0.9300	0.8474	0.8474	0.8923	0.9023	
Specificity	0.7836	0.8090	0.8024	0.7991	0.7998	
Accuracy	0.7968	0.8148	0.7157	0.8114	0.8129	
<b>Grader 3</b>						
<b>Tested on</b>	G1A1	G2A1	G2A2	G3A1	G3A2	
Sensitivity	0.9869	0.9354	0.9637	0.9634	0.9731	
Specificity	0.7603	0.7227	0.7135	0.7100	0.7107	
Accuracy	0.7199	0.7516	0.7436	0.7388	0.7405	

**Table 4.** CNN-based Classification results

<b>Grader 1</b>			
<b>Test Set</b>	<b>Accuracy</b>	<b>Sensitivity</b>	<b>Specificity</b>
G1A2	0.8027	0.6989	0.8482
IOSTAR	0.6479	0.7435	0.6127
<b>Grader 2</b>			
<b>Test Set</b>	<b>Accuracy</b>	<b>Sensitivity</b>	<b>Specificity</b>
G2A2	0.6952	0.5309	0.7642
IOSTAR	0.5456	0.6999	0.4887
G1A1	0.7349	0.5971	0.7953
<b>Grader 3</b>			
<b>Test Set</b>	<b>Accuracy</b>	<b>Sensitivity</b>	<b>Specificity</b>
G3A2	0.7142	0.6117	0.7571
IOSTAR	0.5896	0.7345	0.5363
G1A1	0.7423	0.6204	0.7958

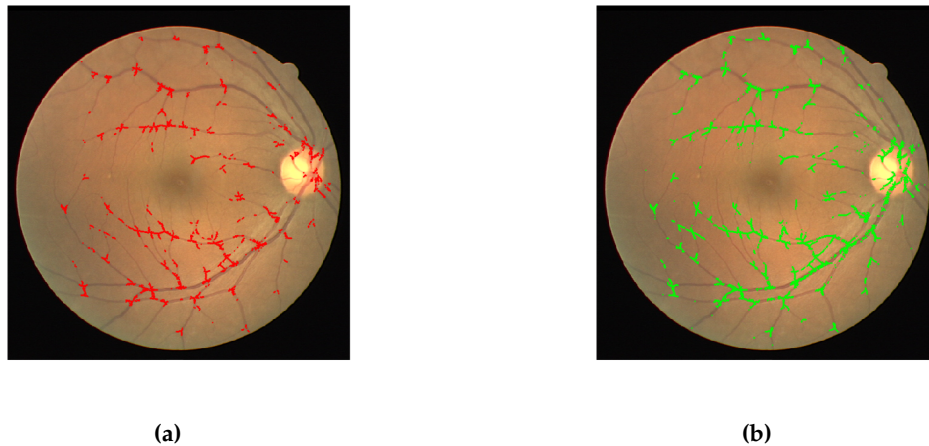
**Table 5.** Confusion Matrices for CNN-based Classification results. BF denotes bifurcations, CR denotes crossings. True labels are along rows, predicted along columns.

Training on Grader 1									
G1A2	BF	CR	IOSTAR	BF	CR				
BF	13289	2068		BF	12375	1907			
CR	2379	4801		CR	7821	5527			
Grader 2									
G2A2	BF	CR	IOSTAR	BF	CR	G1A1	BF	CR	
BF	12250	3158		BF	14430	3262	BF	11468	2547
CR	3780	3574		CR	15095	7607	CR	2951	3775
Grader 3									
G3A2	BF	CR	IOSTAR	BF	CR	G1A1	BF	CR	
BF	12046	2585		BF	15475	2820	BF	11414	2387
CR	3864	4072		CR	13381	7803	CR	2929	3902

**Figure 5.** Example of identifying bifurcations and crossings in fundus images. [20] Reproduced with permission

## 222 4. Discussion

223 We have produced a method that can learn to detect and classify vessel bifurcations and crossings  
 224 using a very small dataset of 40 fundus images that had been manually classified for bifurcations  
 225 and crossings and their type. Using the CNN  $\mathcal{C}_1$ , we managed to detect the bifurcations and crossings  
 226 to an impressive detection accuracy of over 90% due in part to the relatively large amount of patches  
 227 containing bifurcations and crossings. Along with the skeletonisation, our deep learning classification  
 228  $\mathcal{C}_2$  for vessel type gave us a high accuracy. The classifications statistics are similar to that of the



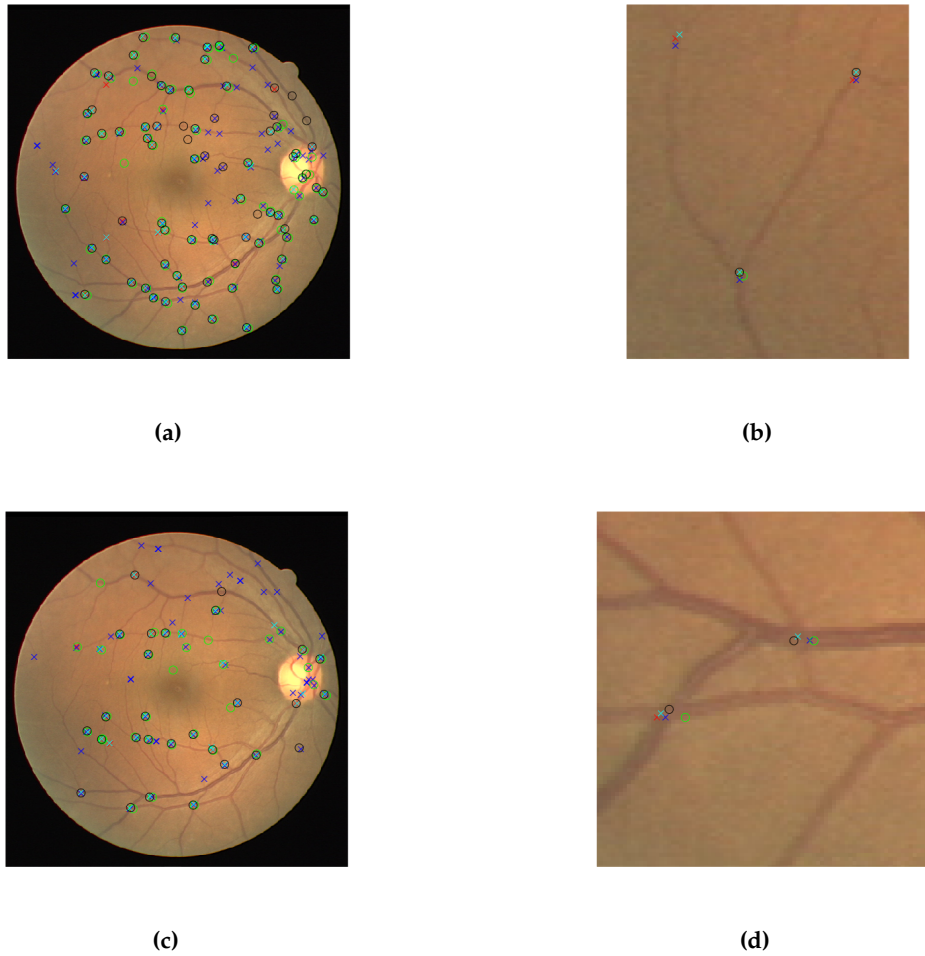
**Figure 6.** These are two examples from the test set that show how the patch classification leads to the building up of a vessel map from identifying and classifying the vessel junctions and reconstructing the classified patches. The detected junctions are shown on the fundus image showing that the algorithm clearly identifies junction points. [20] Reproduced with permission

229 intravariability between graders and hence the method has more chance of reaching higher results  
230 should a consistent grading be given within the patches. This can be seen by the higher testing results  
231 on the third grader. Increasing the size of our dataset would allow better distinction in the classification  
232 of the vessel bifurcations and crossings. It is worth noting that junction type training was undertaken  
233 on a couple of thousand patches and tested on around 800. Through training on more images the  
234 model could be fine tuned to refine the filters and increase distinction accuracy.

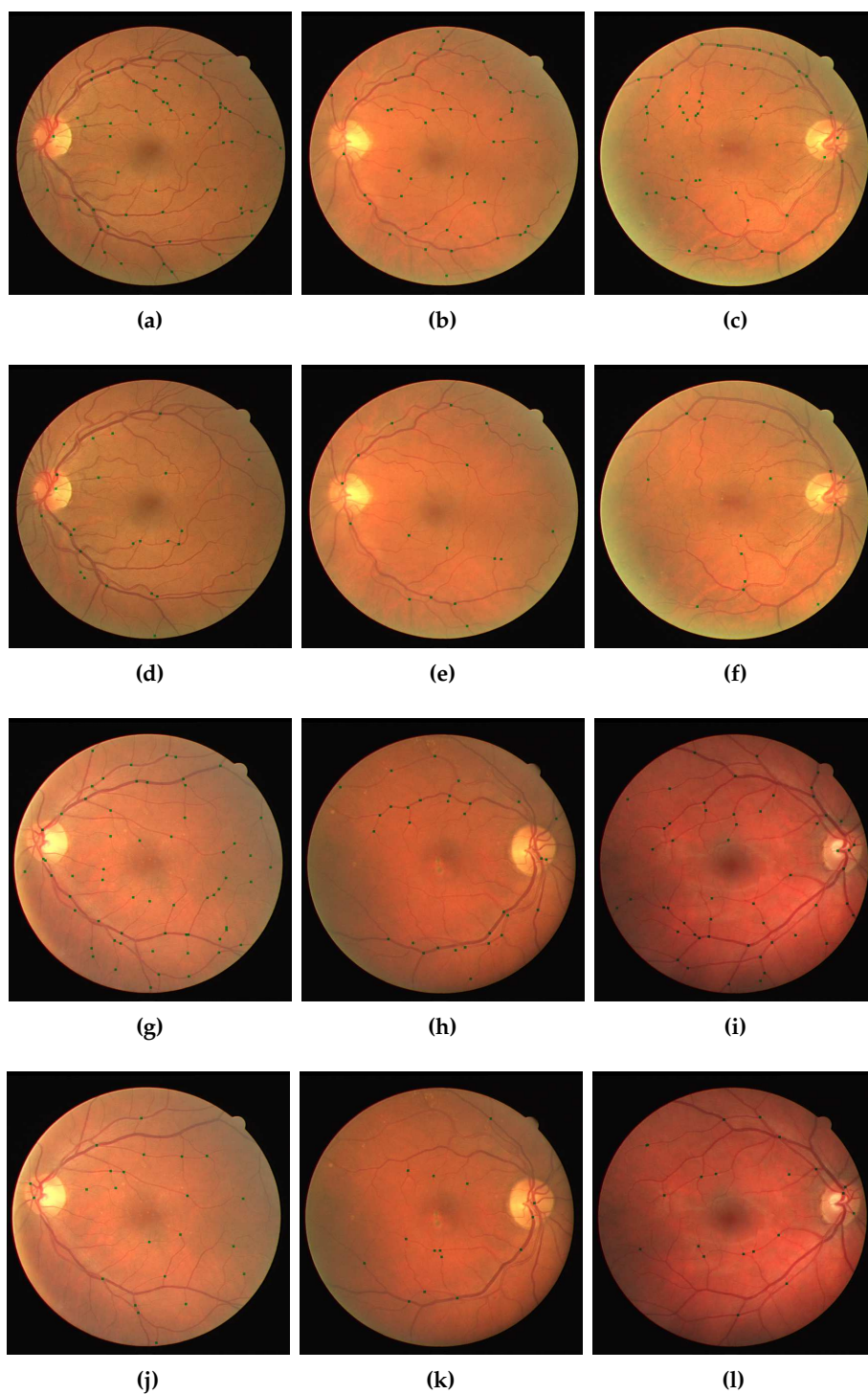
235 The current algorithm works well for images which have been manually segmented but this  
236 time-consuming task could be further extended to incorporate automatic segmentation techniques [3].  
237 A further very useful extension would be to automatically determine whether the artery or vein is in  
238 front given arteriovenous crossings, along with consideration of intra and inter-observer variability.  
239 In order to better identify and classify bifurcations and crossings with other nearby bifurcations and  
240 crossings, it would be useful to consider extending our method to a multi-scale approach. Furthermore,  
241 while we have included images with different vessel pathologies due to diseases such as retinopathy,  
242 using datasets containing other retinal diseases this could be studied further to investigate how this  
243 affects the detection and classification of vessel junctions.

## 244 5. Conclusion

245 The challenging task of detecting and classifying vessel bifurcations and crossings in fundus  
246 images is achieved to a high level of accuracy using our method. The variability over datasets without  
247 training on the dataset represents a robust algorithm for unseen images. The ability to expand on  
248 this method to make the detection both quicker and more accurate than manual classification is  
249 possible. These preliminary results demonstrate that the overall framework, including the deep  
250 learning approach proposed, is a viable technique to accurately find and identifying vessel bifurcations  
251 and crossings with little training data. More extensive testing of this framework could be undertaken  
252 to assess the transferability of these results and patch sizes to different size images from different  
253 datasets. However, there is no reason why this framework would not be directly applicable to another  
254 dataset.



**Figure 7.** (a) and (c) show the identified bifurcations (a) and crossings (c) for an example image from the DRIVE dataset. The results are shown along with the annotations provided by each grader. The annotation of grader 1 is shown by a red x, grader 2 by a blue x and green o, grader 3 by a cyan x and black o. (b) and (d) are zoomed in to demonstrate the negligible difference in the classification of the vessel bifurcation (b) and crossing (d) from the grader's annotations and the consistency in the annotations provided. [20] Reproduced with permission



**Figure 8.** Example of distinguishing between crossings and bifurcations in fundus images. In each column, rows one and three show bifurcations and rows two and four show the crossings for the respective examples. [20] Reproduced with permission

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261

- 262 1. Benjamin, E.J.; Blaha, M.J.e.a. Heart Disease and Stroke Statistics 2017  
 263 Update: A Report From the American Heart Association. *Circulation* **2017**,  
 264 [<http://circ.ahajournals.org/content/early/2017/01/25/CIR.000000000000485.full.pdf>].
- 265 2. MacGillivray, T.; Trucco, E.; Cameron, J.; Dhillon, B.; Houston, J.; Van Beek, E. Retinal imaging as a source  
 266 of biomarkers for diagnosis, characterization and prognosis of chronic illness or long-term conditions. *The*  
 267 *British journal of radiology* **2014**, *87*, 20130832.
- 268 3. Zhao, Y.; Rada, L.; Chen, K.; Harding, S.P.; Zheng, Y. Automated vessel segmentation using infinite  
 269 perimeter active contour model with hybrid region information with application to retinal images. *IEEE*  
 270 *transactions on medical imaging* **2015**, *34*, 1797–1807.
- 271 4. Staal, J.; Abràmoff, M.D.; Niemeijer, M.; Viergever, M.A.; Van Ginneken, B. Ridge-based vessel  
 272 segmentation in color images of the retina. *IEEE transactions on medical imaging* **2004**, *23*, 501–509.
- 273 5. Chutatape, O.; Zheng, L.; Krishnan, S.M. Retinal blood vessel detection and tracking by matched Gaussian  
 274 and Kalman filters. Engineering in Medicine and Biology Society, 1998. Proceedings of the 20th Annual  
 275 International Conference of the IEEE. IEEE, 1998, Vol. 6, pp. 3144–3149.
- 276 6. Gonzalez, R.; Wintz, P. Abbasi-Sureshjani, S and Smit-Ockeloen, I and Bekkers, E and Dashtbozorg, B and  
 277 ter Haar Romeny, B **2016**.
- 278 7. Dashtbozorg, B.; Abbasi-Sureshjani, S.e.a. Infrastructure for Retinal Image Analysis **2016**.
- 279 8. Bekkers, E.; Duits, R.; Berendschot, T.; ter Haar Romeny, B. A multi-orientation analysis approach to retinal  
 280 vessel tracking **2014**.
- 281 9. Fukushima, K. Neocognitron: A self-organizing neural network model for a mechanism of pattern  
 282 recognition unaffected by shift in position. *Biol. Cybern.* **1980**, *36*, 193–202.
- 283 10. Cun, Y.L.; Boser, B.; Denker, J.S.; Howard, R.E.; Habbard, W.; Jackel, L.D.; Henderson, D. Advances in  
 284 Neural Information Processing Systems 2. Citeseer, 1990, pp. 396–404.
- 285 11. Srivastava, N.; Hinton, G.; Krizhevsky, A.; Sutskever, I.; Salakhutdinov, R. Dropout: A simple way to  
 286 prevent neural networks from overfitting. *J. Mach. Learn. Res.* **2014**, *15*, 1929–1958.
- 287 12. Nair, V.; Hinton, G.E. Rectified linear units improve restricted boltzmann machines. Proceedings of the  
 288 27th International Conference on Machine Learning (ICML-10), 2010, pp. 807–814.
- 289 13. Krizhevsky, A.; Sutskever, I.; Hinton, G.E. ImageNet Classification with Deep Convolutional Neural  
 290 Networks. In *Advances in Neural Information Processing Systems 25*; Pereira, F.; Burges, C.J.C.; Bottou, L.;  
 291 Weinberger, K.Q., Eds.; Curran Associates, Inc., 2012; pp. 1097–1105.
- 292 14. Krizhevsky, A. Learning multiple layers of features from tiny images. Technical report, 2009.
- 293 15. Sonka, M.; Hlavac, V.; Boyle, R. *Image processing, analysis, and machine vision*; Cengage Learning, 2014.
- 294 16. Gonzalez, R.; Wintz, P. Digital image processing **1977**.
- 295 17. He, K.; Zhang, X.; Ren, S.; Sun, J. Deep Residual Learning for Image Recognition. *CoRR* **2015**,  
 296 *abs/1512.03385*.
- 297 18. LeCun, Y.; Cortes, C. MNIST handwritten digit database **2010**.
- 298 19. Krizhevsky, A. Learning Multiple Layers of Features from Tiny Images. [https://www.cs.toronto.edu/  
 299 ~kriz/learning-features-2009-TR.pdf](https://www.cs.toronto.edu/~kriz/learning-features-2009-TR.pdf).
- 300 20. Pratt, H.; Williams, B.M.; Ku, J.; Coenen, F.; Zheng, Y., Automatic Detection and Identification of Retinal  
 301 Vessel Junctions in Colour Fundus Photography. In *Medical Image Understanding and Analysis: 21st Annual  
 302 Conference, MIUA 2017, Edinburgh, UK, July 11–13, 2017, Proceedings*; Springer International Publishing:  
 303 Cham, 2017; pp. 27–37.

- 304 21. Abbasi-Sureshjani, S.; Smit-Ockeloen, I.; Zhang, J.; Ter Haar Romeny, B. Biologically-inspired supervised  
305 vasculature segmentation in SLO retinal fundus images **2015**.
- 306 22. Chollet, F. keras. <https://github.com/fchollet/keras>, 2015.
- 307 23. Kingma, D.P.; Ba, J. Adam: A Method for Stochastic Optimization. *CoRR* **2014**, *abs/1412.6980*.

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